

The effect of plasma-treated polyethylene fiber on the fracture strength of polymethyl methacrylate

Van Ramos, Jr., DDS,^a Dennis A. Runyan, DDS, MS,^b and Loren C. Christensen, DDS^c

U.S. Army Dental Activity, Walter Reed Army Medical Center, Washington, D.C., and Dwight David Eisenhower Army Medical Center, Department of Clinical Investigation, Fort Gordon, Ga.

The effect of a plasma-treated polyethylene fiber on the fracture strength of polymethyl methacrylate was evaluated in this study. Sixteen treated and 16 untreated polymethyl methacrylate bars were tested by use of a three-point compression loading apparatus. Under the conditions of this experiment the treated bars showed a mean fracture strength of 12.56 MPa compared with 9.81 MPa for the untreated samples. In addition to the increased fracture strength, the treated bars also demonstrated resistance to crack propagation. The bars remained in one piece, held together throughout the compression loading by the polyethylene fiber. The clinical implication of these findings is a reduced incidence of fixed provisional restoration failure. (J Prosthet Dent 1996;76:94-6.)

In clinical situations a fixed partial denture (FPD) may be subjected to a variety of forces. El-Ebrashi et al.¹ reported that the force on an FPD includes compression at the point of load application and tension and shear force at points that resist the load. Because provisional restorative materials have inherent weaknesses, any method that would effectively add strength is welcomed.² Fracture strength of these materials has been increased as a result of the decrease in the size and number of porosities in the polymerized product under the influence of pressure.³ Also, metal, carbon-graphite, sapphire, silane-treated glass, and polyethylene (PE) have all been used with varying degrees of success.⁴⁻¹⁰ Long-term use of fixed provisional restorations has been suggested in implant hybrid cases in which periodontally involved abutments are retained for a period of time to allow osseointegration of implants.¹¹ These fixed provisional restorations will reduce transmucosal loading during the healing phase and therefore improve long-term prognosis.² In this situation a provisional restoration that is less susceptible to fracture would be beneficial.

The purpose of this study was to determine the effect on

fracture strength of polymethyl methacrylate (PMMA) reinforced with a plasma-treated PE fiber that is 0.4 mm thick and manufactured in various widths and lengths.

METHODS AND MATERIAL

One type of autopolymerizing PMMA (Jet, Lang Dents Mfg. Co., Inc., Wheeling, Ill.) was tested for flexure strength with and without the woven PE fiber (Ribbon Inc., Seattle, Wash.). A silicone mold (Extrude, Kerr Mfg. Romulus, Mich.) and a vacuum-formed matrix was used to make 32 resin specimens measuring 60 × 5 × 5 mm. Sample size was determined by use of an a priori α of 0.05 and β of 0.20 with a minimal clinical significance of 5%. The mold was marked at a point two thirds from the base. This marking was used to control the placement of the fiber into the unpolymerized resin so that during testing the fiber would be placed under tension.

At a 2.5:1 polymer-to-monomer ratio all the specimens were made by mixing the polymer-monomer and pouring the resultant mixture into the silicone mold. This mixture was used in a previous study,¹⁰ and it provided a smooth consistency for incorporating the PE fiber. The vacuum formed matrix was then placed over the mixture, secured with a rubber band, and allowed to polymerize in a pressure bath at 110° F and 20 pounds per square inch. Sixteen specimens had the PE fiber added to the mixture when the mold was two thirds full. The remainder of the mold was then filled, covered, and allowed to polymerize in the pressure pot. A 4 mm wide fiber was selected and cut to a length of 60 mm. When the polymerized specimen was removed from the mold, it was examined to determine whether the two-third mark was visible on its side (Fig. 1). In this way the specimen could be properly placed in the testing apparatus with the material away from the point of compression. According to the manufacturer, Ribbon PE fiber has been reported to increase fracture strength of resins when it is placed on the tension side. The specimens were stored

The opinions or assertions contained herein are the private views of the authors and are not to be construed as official or as reflecting the views of the Department of the Army or the Department of Defense. Identification of commercial materials and equipment does not imply official recommendation or endorsement or that the materials and equipment are necessarily the best available for the purpose.

Presented at the National Capitol Area Section of the American College of Prosthodontics, February 1994.

^aMajor, Dental Corps, Senior Resident Advanced Education Program in Prosthodontics, Walter Reed Army Medical Center.

^bColonel, Dental Corps, Department of Clinical Investigation, Fort Gordon.

^cColonel, Dental Corps, Director, Advanced Education Program in Prosthodontics, Walter Reed Army Medical Center.

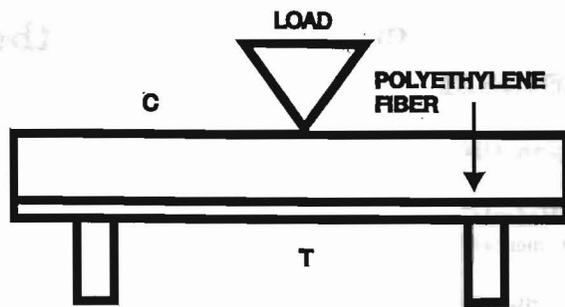


Fig. 1. Diagrammatic representation of destruct test, resultant forces, and positioning of PE fiber to resist tension. C, Compression; T, tension.

in normal saline solution at room temperature for 12 to 24 hours before testing.

Each specimen was loaded with an Instron testing machine (Instron Corp., Canton, Mass.) with a crosshead speed of 5 mm per minute. The force required to fracture the specimens was noted. The test specimens were placed under the load cell so that a central area of 20 mm was loaded and it was unknown which samples were treated and which were not treated with the PE fiber. Treated and untreated fractured specimens were examined under a scanning electron microscope. No porosities were noted in any of the samples. The data were analyzed with a two-sample *t* test.

RESULTS

The mean experimental values and SDs are illustrated in Figure 2. The difference in the mean values between the two groups is greater than would be expected by chance. The mean value of the force required to cause a fracture in the untreated samples was 9.81 MPa, and the mean value for the treated sample was 12.56 MPa. A *t* test between the two groups revealed a statistically significant difference ($p < 0.001$).

DISCUSSION

Treating a polymer with plasma can increase its surface energy by modifying the chemistry of its surface.¹² Plasma is a partially ionized gas that contains ions, electrons, and other neutral species at many different energy levels. When energized by an electrical field, free radicals, ions, and atoms are formed that can interact with solid surfaces that have been placed in the plasma. This results in modifications of the surface chemistry of the solid. In this situation the solid is the PE woven fiber. The increase in surface energy is responsible for the greater chemical reactivity and compatibility with other materials.¹²

Larson et al.¹⁰ found the use of carbon graphite to be promising for the reinforcement of long-span provisional FPDs; however, the poor esthetic result was a major drawback. On the other hand, PE is virtually invisible once incorporated into the PMMA.

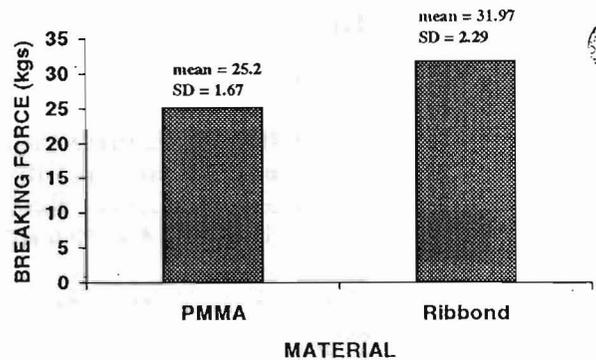


Fig. 2. Comparison of mean fracture strengths of treated and untreated PMMA bars.

One of the interesting outcomes of this experiment was that the treated PMMA bars would not be a catastrophic failure. In fact, a crack would occur on the tension side but would not propagate through to the compression point. The embedded fiber could not be stretched enough for the crack in the resin to continue. The fiber appeared to hold the two pieces together. Because a fracture failure is usually related to the initiation of a crack and its subsequent propagation until displacement,¹³ a complete failure with the embedded fiber may not occur. If a provisional FPD fractures in the mouth, it is difficult if not impossible to pair. This presents an inconvenience to both the dentist and the patient because the provisional prosthesis must often be refabricated. If a fracture occurs in the resin with the plasma-treated PE reinforcement, the repair would be simpler because the fractured joint could easily be approximated and repaired.

In this study scanning electron micrographs were inconclusive regarding whether a bond occurred between the PMMA and the Ribbond PE fiber. The increase in fracture strength and resistance to crack propagation may be attributed to an actual chemical bond, mechanical interlocking of the PMMA to the fiber, or both.

Use of the fiber is simple; however, there are some handling requirements. When PMMA is used, the fiber must first be wetted with the monomer before it is placed in the mixture of monomer and polymer. To avoid contamination of the plasma-treated surface, a pair of cotton gloves are provided in the package, along with a pair of scissors designed for cutting the fiber to the required length.

CLINICAL IMPLICATION

Repairing or remaking provisional restorations can be a time-consuming endeavor. The added strength of the PMMA with the fiber can reduce clinical failures of provisional FPDs. Esthetics are not compromised if used in the anterior region because the fiber becomes invisible once incorporated into the PMMA.

SUMMARY AND CONCLUSION

Provisional restorations made with PMMA are strengthened by the addition of this plasma-treated PE fiber. The fiber is simple to place into the acrylic resin, although there are some handling requirements to prevent contamination of the plasma treatment. No attempt was made to vary the monomer/polymer ratio to see what effect this might create with the incorporation of the fiber. This study attempted to standardize samples and to focus on the effect of the addition of Ribbond PE fiber. Follow-up studies could examine this variation, differences in cross-sectional design, or the relation of the width of the fiber to the width of the specimen.

REFERENCES

1. El-Ebrashi MK, Craig RG, Peyton FA. Experimental stress analysis of dental restorations, VII: structural design and stress analysis of fixed partial dentures. *J Prosthet Dent* 1970;23:177-86.
2. Jendresen MD, Allen EP, Bayne SC, Hansson TL, Klooster J, Preston JD. Report of the Committee on Scientific Investigation of the American Academy of Restorative Dentistry. *J Prosthet Dent* 1992;68:137-90.
3. Donovan TE, Hurst RG, Campagni WV. Physical properties of acrylic resin polymerized by four different techniques. *J Prosthet Dent* 1985;54:522-4.
4. Sehajpal SB, Sood VK. Effect of metal fillers on some physical properties of acrylic resin. *J Prosthet Dent* 1989;61:746-51.
5. Schreiber CK. Polymethylmethacrylate reinforced with carbon fibers. *Br Dent J* 1971;130:29-30.
6. Manley TR, Bowman AJ, Cook M. Denture bases reinforced with carbon fibers. *Br Dent J* 1979;146:25-9.
7. Ruyter IE, Ekstrand K, Bjork N. Development of carbon/graphite fiber reinforced poly (methylmethacrylate) suitable for implant-fixed dental bridges. *Dent Mat* 1986;2:6-9.
8. Grant AA, Greener EH. Whisker reinforcement of poly methyl methacrylate denture base resins. *Aust Dent J* 1967;12:29-33.
9. Solnit GS. The effect of methyl methacrylate reinforcement with silane-treated and untreated glass fibers. *J Prosthet Dent* 1991;66:310-4.
10. Larson WR, Dixon DL, Aquilino SA, Clancy JM. The effect of carbon graphite fiber reinforcement on the strength of provisional crown and fixed partial denture resins. *J Prosthet Dent* 1991;66:816-20.
11. Meffert RM, Langer B, Fritz ME. Dental implants: a review. *J Periodontol* 1992;63:859-70.
12. Kaplan SL, Rose PW. Plasma surface treatment of plastics to enhance adhesion: an overview. Belmont, CA: Plasma Science, 1990. (Publication no 9.)
13. Gegauff AC, Pryor HC. Fracture toughness of provisional resins for fixed prosthodontics. *J Prosthet Dent* 1987;58:23-9.

Reprint requests to:

DR. DENNIS A RUNYAN
DEPARTMENT OF CLINICAL INVESTIGATION
EAMC, BLDG. 332
FORT GORDON, GA 30905
10/1/72588